



## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

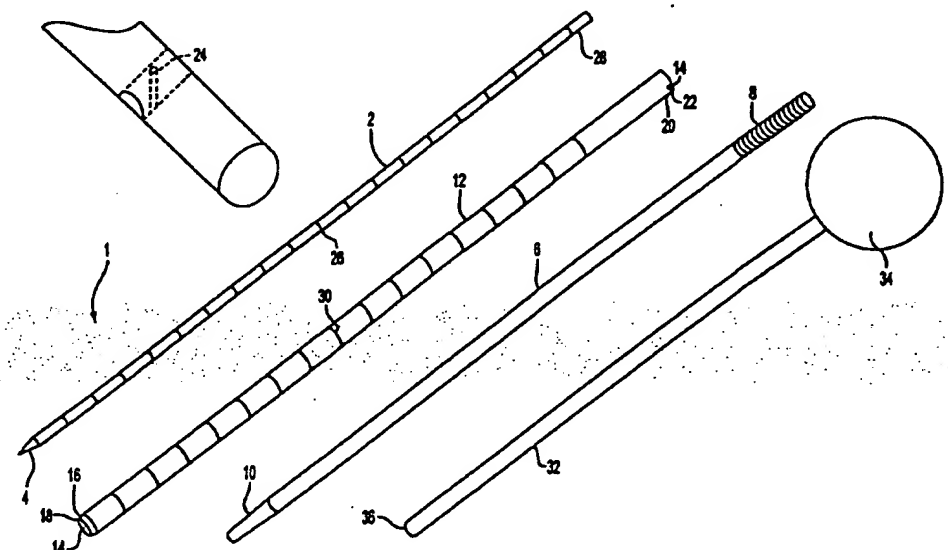
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<b>(21) International Application Number:</b> PCT/US00/06643 <b>(22) International Filing Date:</b> 15 March 2000 (15.03.2000) <b>(30) Priority Data:</b> 09/525,008 14 March 2000 (14.03.2000) US 60/124,661 16 March 1999 (16.03.1999) US 60/133,276 10 May 1999 (10.05.1999) US 60/167,017 23 November 1999 (23.11.1999) US <b>(60) Parent Application or Grant</b> BHATNAGAR, Mohit [/]; O. MAJOR, Eric [/]; O. BHATNAGAR, Mohit [/]; O. MAJOR, Eric [/]; O. MCQUADE, Paul, F.; O.	<b>Published</b>	
<b>(54) Title: APPARATUS AND METHOD FOR FIXATION OF OSTEOPOROTIC BONE</b> <b>(54) Titre: APPAREIL ET PROCEDE DE FIXATION D'OS OSTEOPOROTIQUEONE</b>  <b>(57) Abstract</b> <p>A Novel surgical apparatus and method of use in osteoplasty and other methods of injecting materials into a subject for medical purposes. The present invention particularly relates to the surgical treatment of traumatic, pathogenic, or osteoporotic bone conditions of the human and other animal body systems and more particularly, to a novel apparatus and method for injection of a material into a lesion of a vertebral body or other bony structure.</p> <b>(57) Abrégé</b> <p>L'invention concerne un nouvel appareil chirurgical et un procédé correspondant utilisés en ostéoplastie. L'invention concerne également d'autres procédés permettant d'injecter des matières chez un patient à des fins médicales. La présente invention concerne notamment le traitement chirurgical d'états osseux traumatiques, pathogènes ou ostéoporotiques d'organismes humains et animaux. L'invention concerne plus particulièrement un nouvel appareil et un procédé permettant l'injection d'une matière dans une lésion du corps d'une vertèbre ou d'une autre structure osseuse.</p>		

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(21) International Application Number: PCT/US00/06643 (22) International Filing Date: 15 March 2000 (15.03.00) (30) Priority Data: 60/124,661 16 March 1999 (16.03.99) US 60/133,276 10 May 1999 (10.05.99) US 60/167,017 23 November 1999 (23.11.99) US 09/525,008 14 March 2000 (14.03.00) US (63) Related by Continuation (CON) or Continuation-in-Part (CIP) to Earlier Application US 09/525,008 (CIP) Filed on 14 March 2000 (14.03.00) (71)(72) Applicants and Inventors: BHATNAGAR, Mohit [US/US]; 18712 Severn Road, Gaithersburg, MD 20879 (US). MAJOR, Eric [US/US]; 21157 Cavalier Court, Asburn, VA 20147 (US). (74) Agents: MCQUADE, Paul, F. et al.; Pillsbury Madison & Suto LLP, 1100 New York Avenue, N.W., Washington, DC 20005 (US).		(81) Designated States: AE, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CR, CU, CZ, DE, DK, DM, DZ, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, TZ, UA, UG, US, UZ, VN, YU, ZA, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SL, SZ, TZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).  Published With international search report.	
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**Description**

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## APPARATUS AND METHOD FOR FIXATION OF OSTEOPOROTIC BONE

This invention relates to a novel surgical apparatus for use in osteoplasty and other methods of injecting materials into a subject for medical purposes. Particularly, the present invention relates to the surgical treatment of traumatic, pathogenic, or osteoporotic bone conditions of the human and other animal body systems and more particularly, to a novel apparatus and method for injection of a material into a lesion of a vertebral body or other bony structure.

### BACKGROUND

Lesions within the bone can result from osteoporosis, tumor, or other pathogenic causes. Most common among the elderly population is the degenerative effect of osteoporosis, particularly the female elderly. Osteoporosis is mediated at least in part by genetic defects and a fall in circulating estrogen levels. Although calcium replacement therapy can have some beneficial effects, the larger doses of calcium involved have other less helpful consequences and accordingly, the prognosis for those with bone demineralization is not particularly good. Of great concern is the fact that every year in the United States there occurs approximately 1.2 million bone failures due to osteoporosis. Vertebral compression failures are a major orthopedic health concern of the elderly due to the long term debilitating nature of the injury.

Historically, osteoporotic vertebral body compression failures have been treated with bed rest, analgesics, and intravenous hydration during the first week after onset of the problem. These steps are followed by the prescription of a soft or firm spinal corset, depending upon the physician's preference. In most cases the corset is

5 not worn because the patient suffers much discomfort and oftentimes greater  
discomfort than that due to the failure of the vertebral body. In any case, this  
10 conventional approach required extensive hospitalization and bed rest, which often  
results in very limited success, chronic pain, and further osteoporosis with worsening  
5 conditions of the vertebral body. The costs associated with such extended  
hospitalization and the negative effect on the general health of the patient from such  
15 prolonged inactivity should be avoided if possible.

Traditional surgical techniques employed to alleviate vertebral compression  
20 failures can involve major invasive surgical techniques with all of the possible  
negative consequences. Such techniques have typically required prolonged patient  
10 recuperation and unfortunately have met with limited success in alleviating pain and  
returning the patient to a normal life style.  
25

More recently efforts have been made to develop surgical techniques for repair  
30 of vertebral compression failures of osteoporotic bone by using conventional  
instruments in a transpedicular approach to penetrate the vertebral body, including a  
15 standard syringe, and then inject a flowable synthetic bone material or bone cement  
directly into the vertebral body through the syringe. This technique of vertebroplasty  
35 requires that the physician take the utmost care to avoid damage to the spinal cord  
when drilling through the narrow dimensions of the pedicle of the vertebrae. To  
40 avoid potentially catastrophic results physicians practicing conventional  
20 vertebroplasty require the use of CAT scanning, biplane fluoroscopy, magnetic  
resonance imaging, or other imaging devices to ensure the proper alignment of the  
45 instruments, which bore through and are passed through the narrow pedicle. The  
availability of CAT scanning or sophisticated biplane fluoroscopy in surgical  
50 procedures is limited due to the additional cost associated with equipping surgical  
25

5 suites with the necessary equipment. Further, to protect against accidental damage to  
the spinal cord during the conventional transpedicular approach to the vertebral body,  
the patient is typically placed in a restraining device and stereotaxic procedures are  
10 used to guide the physician's drill and cannula through the pedicle. Due to the  
5 extraordinary care and precision required in conventional vertebroplasty, the time  
needed to complete the surgery and the cost associated with the procedure can be  
15 extensive. Further, general anesthetic is not recommended due to the close proximity  
of the physician's instruments to the spinal cord and the associated need to  
20 communicate with the patient. This requirement, however, also causes concern of  
10 movement of the patient during the surgery; movement which could have serious  
consequences should the spinal cord be damaged as a result. Scholten et al. in U.S.  
25 Patents 4,969,888 and 5,108,404 teaches the conventional surgical technique of  
vertebroplasty with the additional step of employing a balloon as an expansion device  
within the body of the vertebrae to compact the osteoporotic cancellous bone away  
30 from the center and against the walls of the vertebral body. This additional step to  
15 conventional vertebroplasty, taught by Scholten et al., is intended to provide  
additional space within the vertebral body to accept the flowable bone cement through  
35 the needle (syringe). While the conventional vertebroplasty technique using  
conventional surgical apparatus has the distinct disadvantage of drilling through the  
40 pedicle with the potential risk of damage to the spinal column, this additional balloon  
20 expander employed in the process of Scholten et al., provides an additional  
disadvantage by compressing the naturally present internal matrix of the osteoporotic  
45 vertebra against the wall of the vertebral body. Absent this natural matrix, the  
injection of bone cement into the cavity created by the compressing step results in the  
25 formation of an unstructured bolus of bone cement in the center of the vertebral body.

5 Because of the compression of cancellous bone, which as a result lines the walls of  
the vertebra, the bone cement which is infused into the vertebral body does not make  
a strong, direct, bonding contact with the vertebral wall, thus resulting in a potentially  
10 weaker post-surgery vertebral body.

5 There is, therefore, a great need for a surgical technique and associated  
instrumentation by which osteoporotic bone can be safely, expeditiously and  
15 efficiently treated. There is a particular need for a vertebroplasty procedure and  
associated instrumentation which provide a safer, faster procedure that ultimately  
results in a repair to the osteoporotic vertebral body wherein the injected material  
20 does not disturb the natural matrix of the cancellous bone, which along with direct  
contact to the vertebral wall provides a strong, composite matrix. The present  
invention provides an apparatus and a method of percutaneous bone failure fixation,  
25 which satisfies these needs.

#### 30 15 SUMMARY OF THE INVENTION

The process and apparatus of the present invention can be generally used to  
perform osteoplasty, that is the introduction of any injectable material into any of the  
35 bones or tissues of the body. The present invention is particularly suitable for  
injecting materials into bones which have or are susceptible to compression failure  
due to lesions within cancellous bone. More particularly, this invention relates to a  
40 method and apparatus, involving the injection of materials for the fixation of lesions  
or failures of bones, particularly as a result of osteoporosis, tumor, other pathogenic  
conditions or trauma. The invention is especially suitable for use in the vertebroplasty  
45 procedures, such as, the fixation or prevention of vertebral body compression failures,  
25 although the instrumentation and methods of the present invention can be used for a



5 wide variety of osteoplasty procedures, such as, failures or lesions in bones  
throughout the body.

10 An object of the present invention is to provide an apparatus, which is useful  
for the surgical procedure of safely introducing a material into a lesion or space within  
5 or around a bone or tissue.

15 Another object of the present invention is to provide a surgical method for  
safely introducing an injectable material into a lesion or space within or around a bone  
or tissue.

20 More particularly, it is an object of the present invention to provide an  
apparatus, which is sized and configured to safely contact or breach the cortical bone  
10 and establish an introducing channel through the apparatus and through the cortical  
bone into the cancellous bone through which a material can be introduced. The  
25 material introduced into the interior of the bone can be any biocompatible or  
therapeutic materials, such as, for example, antibiotics, whole cellular implants,  
30 15 natural products of cells, recombinant nucleic products, protein products of  
recombinant cells, allograft or autograft bone, bone cement products as are well  
known in the art (such as polymethylmethacrylate and the like), or any other flowable  
35 material useful for therapeutic, prosthetic, or bone strengthening purposes.

40 Another object of the present invention to provide an apparatus, which is sized  
and configured to be used by a physician to safely introduce a material into the  
cancellous bone of a vertebral body. In the surgical procedure of the present  
invention the apparatus can introduced by direct vision, open or percutaneously,  
45 laproscopically, thorascopically, or by open surgical procedures. The apparatus can  
be introduced into the vertebral body by a variety of approaches, to include, for  
25 example, postero-lateral and lateral and/or bilateral percutaneous approaches and a

transpedicular approach. Such introduction of the apparatus can be accomplished with or without the conventional requirement for CAT scanning or sophisticated biplane fluoroscopy and further can be performed safely using general or local anesthetic. No irrigation, evacuation, or use of cancellous bone expanders is required for the successful use of the apparatus to introduce the material into the interior of the vertebral body.

Additionally, an object of the present invention is to provide a modular pedicle finder, which facilitates the placement of an instrument for penetrating the pedicle of a vertebra.

#### BRIEF DESCRIPTION OF THE DRAWINGS

The invention will now be described, by way of illustration only, with reference to the accompanying drawings.

FIG. 1 is an isometric view of the components of the one embodiment of the apparatus of the present invention.

FIG. 2 is an isometric view of the assembled Guide wire and Aligning Cannulae of the present invention.

FIG. 3 is an isometric view of the assembled Delivery cannulae and Plunger of the present invention.

FIG. 4 depicts the present invention equipped with an optional syringe system.

FIG. 5 is a depiction of a guide wire that can be used in the present invention having a Luer lock for providing a fluid tight attachment to an infusion device or syringe.

5 FIG. 6 is a depiction of a delivery cannulae that can be used in the present invention, which is configured to be capable of receiving the guide wire shown in FIG. 5.

10 FIG. 7 is a depiction of the assembled guide wire and delivery cannulae shown in FIGs. 5 and 6.

15 FIG. 8 is a depiction of a handle configured to be capable of removable attachment to the Luer lock of the guide wire shown in FIG. 5 or the cannulae shown in FIG. 6.

20 FIG's. 9A-C are detail views of the handle shown in FIG. 8.

10 FIG. 9D is a depiction of an embodiment of the handle shown in FIG. 8 which is configured with a removable proximal end for purposes of exposing the proximal end of the guide wire for ease in movement, insertion, and extraction from the delivery cannulae. FIG. 9E-F shows examples of some of the alternative end attachments, which can be employed with the handle shown in FIG. 9D. FIGS. 9H-G depict a cannulated T-handle which can be used with the present invention. FIG. 9I is a partial sectional view of an alternative embodiment of the present invention employing a handle having a removable proximal end, which acts as an extended impact surface.

35 FIG's. 10A-B are cross-sectional side (10A) and end (10B) views of the plunger shown in FIG. 10C, which can be used with the apparatus of the present invention. FIG. 10C is a depiction of the plunger assembly, which includes the handle shown in FIG's. 10A-B. FIGS. 10D-J are various views of an alternative embodiment of a plunger that can be used with an embodiment of the present invention employing a threaded plunger and cannulae.

45 FIG. 11A is a depiction of a hand operated plunger actuator which can be used with the apparatus of the present invention. FIG. 11B is a depiction of a type of

5 syringe which can be used to contain a material for use in the method of the present  
invention, the syringe being an example of the type syringe which can be used with  
the hand operated plunger actuator shown in FIG. 11A. Unlike other plunger  
10 actuators, this plunger actuator of the present invention allows for controlled  
injection down to 1 cc of material per squeeze by the operator. FIGS. 11C-E are  
15 depictions of an alternative multilumen-type cannulae which can be used to contain  
more than one material for simultaneous or sequential injection in the method of the  
present invention.

20 FIG. 12A is a depiction of an application of the method of the present  
invention, which employs a flexible cannulae for delivery of a material into the bone  
material of a joint, such as, for example into the acetabulum.

25 FIG. 12B is an enlarged cross-sectional depiction of the flexible cannulae  
shown in FIG. 12A showing an example of a mechanism which can be employed to  
steer the flexible cannulae. The plunger technology depicted in FIG. 10 maintains a  
30 flexible shaft for delivery through the flexible lumen of the flexible cannulae.

15 FIG's. 13A-B show a specialized impact forceps, which can be used with the  
device of the present invention for purpose of facilitating the entry of the device into  
35 the bone.

FIG. 14 and FIG. 15 are depictions of a conventional prior art method of  
20 vertebroplasty. FIG 14. shows a transpedicular approach to the vertebral body. FIG.  
15 shows the deep penetration of the vertebral body using a transpedicular approach.

45 FIG. 16 is a depiction of the apparatus of the present invention positioned  
relative to a sectional view of a vertebral body during operation of the method of the  
preferred embodiment of the present invention.

5           FIG. 17 is a depiction of a first alternative embodiment of the method of the  
present invention showing a bilateral approach to the vertebra. Such a bilateral  
approach would preferably be done in order of first one side and then the other,  
10           although the figure depicts both steps simultaneously.

5           FIG. 18 is a depiction of a second alternative embodiment of the method of the  
present invention in which the cancellous bone is penetrated with minimal disruption  
15           of the cancellous bone to permit more extensive infusion of the injectable material.

#### 20           DETAILED DESCRIPTION

10           The apparatus and method of the present invention can be adapted for use in  
the introduction of any material into any bone that contains a lesion or sufficient  
porosity to accept the materials. The employment of the apparatus and surgical  
25           procedure of the present invention in vertebroplasty, particularly to treat vertebral  
compression failures which result from osteoporotic conditions is herein described  
30           below as illustrative of the present invention.

          The following description of the device of the present invention relates to  
FIG'S. 1-3. The apparatus of the present invention is an intraosseous injection device  
35           generally shown at 1. One object of the present invention is to use the injection  
device 1 in a surgical procedure for the safe, effective introduction of materials into a  
20           lesion within a bone, whereby the procedure includes the introduction of a first guide  
wire 2 having a tapered end 4 for effectively breaching the dense compact bone, for  
example, the cortical bone of the vertebra. An aligning cannulae 6 is configured and  
45           sized to easily pass over the first guide wire 2 and when passed down the shaft of the  
guide wire 2 serves as a soft tissue protective sleeve from the point of entry of the  
25           apparatus into the body to the contact point at the exterior surface of the bone being

5 treated. The aligning cannulae 6 has a blunt first end 8 which has a textured surface to facilitate handling and a tapered second end 10 which during operation of the instrument is brought into contact with the bone being treated.

10 A delivery cannulae 12, which is sized and configured to easily pass over the aligning cannulae 6 is inserted over the aligning cannulae 6 for purpose of providing a material conduit 14 through which the injectable material can be introduced into the bone being treated. The delivery cannulae 12 is configured at the delivery cannulae distal end 16 to have a securing edge 18 which serves to hold the delivery cannulae 12 in place on the outer surface of the bone being treated. The delivery cannulae proximal end 20 is configured to have a handle retention member 22, which serves to releasably secure a handle member 24 to the delivery cannulae 12. The handle member 24 can be used for insertion of the delivery cannulae 12 over the aligning cannulae 6 and for improving the grip of the user when placing the securing edge 18 of the delivery cannulae 12 firmly into position on the outer surface of the bone being treated. The removable handle member 24 also can be useful at a later step of the surgical procedure for providing a secure grip, which may be necessary to disengage the delivery cannulae 12 from the surface of the bone prior to extracting the device 1 from the body of the patient. The surface of the delivery cannulae can be provided with graduated indicia 30 which provide depth of penetration information during insertion by the user.

20 The guide wire 2 can be provided with graduated guide wire indicia 26 which extend from the tapered end 4 to the more proximal guide wire blunt end 28. The guide wire indicia 26 provides a means by which the user can easily determine the depth of insertion of the guide wire 2 into the patient during the surgical procedure of the present invention.

5 A plunger member 32 can be provided with an ergonomically configured gripping member 34 at a first end which is used by the user to exert pressure on the plunger member 32 as it snugly passes through the material conduit 14 of the delivery cannulae 12. The second end of the plunger member 32 is configured to have a blunt smooth tip 36. The fit of the plunger member 32 within the material conduit 14 of the delivery cannulae 12 is such that easy sliding engagement of the plunger is permitted without allowing the passage of the injectable material proximally past the blunt smooth tip 36. Further, the plunger member 32 is sized diametrically to provide a fit within the material conduit 14 so as to permit the release of air proximally past the plunger while maintaining the PSI of the injected material as the plunger forces the material distally through the outer cannulae and into the subject. The user can, upon exerting force against the gripping member 34, displace the plunger member 32 through the length of the material conduit 14 of the delivery cannulae 12 and, in doing so, displace any preloaded injectable material out of the distal end of the material conduit 14, through the breach formed by the tapered end 4 of the guide wire 2 and into the interior of the bone being treated.

Alternatively, the movement of the material through the material conduit 14 and into the cancellous bone of the vertebrae could be accomplished by means of a syringe system, generally shown in FIG. 4, at 38. The syringe system of the present invention can include a fluid connector 40, such as, for example, a conventional Luer lock, a bayonet fitting, a hydraulic quick disconnect fitting, or any other fluid tight fitting as is well known in the art. The fluid connector 40, which would be attached to the delivery cannulae 12 and in fluid tight communication with the material conduit 14 can be attached directly to a syringe 42, to a syringe via a flexible conduit 44, or alternatively to an automated infusion device as is well know in the art (not shown).

5 The syringe system 42 can be provided with a syringe plunger tip 42a, which can  
include one or multiple sealing rings diametrically sized to slidably move within the  
syringe 42 in a manner conventional to syringes but with one or more air passages  
10 42b to allow the proximal flow of air past the plunger tip 42a while the plunger tip  
42a forces the material distally through and out of the syringe 42a. The air passages  
15 42b are sized to permit the flow of air but not the flow of the injectable material in a  
proximal direction within the syringe 42. Further, the air passages 42b can be  
arranged on one or more than one annular rings 42c on the plunger tip 42a. When  
20 multiple air passages 42b are arranged on multiple annular rings 42c, it is preferred  
10 that the air passages 42b through one annular ring 42c are offset from the air passages  
42b from an adjacent annular ring 42c. The fluid connector 40 can be attached to the  
25 delivery cannulae 12 in approximate alignment to the longitudinal axis of the delivery  
cannulae 12, at right angles to the longitudinal axis of the delivery cannulae 12, or at  
any position or any angular arrangement to the delivery cannulae 12, which will  
30 15 permit fluid flow through the connector into the material conduit 14.

In the process of the present invention, the mixing of the injectable material,  
such as bone cement, could be accomplished within the syringe system.

35 Another alternative mode of operation would permit the movement of the  
plunger can be automated by attachment of an electro-mechanical or pneumo-  
20 mechanical servo mechanism which would be under control of the physician.

40 Without departing from the concept of the present invention presented in  
Figures 1-4, alternative embodiments of the intraosseous injection device and  
45 peripheral elements as shown in FIG's 5-12B can be provided for use in the method  
of the present invention.



5 As best shown in FIG. 5, a locking guide wire 46, having an attached  
longitudinally aligned male Luer lock 48 and female Luer lock 50 can be provided for  
use with a corresponding alternative delivery cannulae 52, the locking guide wire  
10 having corresponding guide wire connectors 54. FIG. 7 shows the alternative delivery  
cannulae 52 assembled with the locking guide wire 46. FIG. 8 shows a locking guide  
5 wire handle 56, which can be secured to the locking guide wire by the Luer lock 48.

15 As best shown in FIG's. 9A-C, the locking guide wire handle 56 defines a  
longitudinal lumen 58, which is sized and configured to permit passage of the locking  
guide wire 46 as well as the larger cross dimension diameter of the delivery cannulae  
20 52. The guide wire handle 56 can be provided with a view slot 60, which may be  
equipped with a magnifying or non-magnifying clear cover (not shown). The viewing  
slot 60 is sized and configured in the guide wire handle 56 to permit the user to view  
25 the graduated guide wire indicia 26 during operation of the present invention. The  
ability to view the guide wire indicia 26 during operation of the present invention  
30 15 provides a safety feature, which permits the operator to know the depth of insertion of  
the subsequently positioned aligning cannulae and/or outer cannulae. The guide wire  
handle 56 can define a first clearance hole 62, which provides cross access to the  
35 longitudinal lumen 58 and has an orifice diameter sized and configured to correspond  
to the guide wire 46 and can be used to help drive the aligning cannulae into position.  
20 The guide wire handle 56 can be similarly configured to define a second clearance  
40 hole 66, which serves much the same function as the first clearance hole with the  
exception that the second clearance hole is sized and configured to assist in the  
45 insertion of the large delivery cannulae 52. The impact connector element 64 can be  
provided in cross-sectional diameters, which correspond to either the first clearance  
25 hole 62 or the second clearance hole 66. The handle distal end 68 can be provided

5 with a handle Luer connector 70 which corresponds to connectors 54 of the  
alternative delivery cannulae 52, thus providing a secure, quickly released connection  
10 between the guidewire handle 56 and the alternative delivery cannulae 52. An  
enlarged cross-sectional view of the handle Luer connector 70 is shown in FIG. 9B.

5 Although the Luer type connection disclosed in detail is the preferred means of  
providing the handle connection described above, it is within the concept of the  
15 present invention to provide the handle connection using any known connection  
means, such as, for example, other threaded connections, snap-fit connections, cotter-  
pin connections, friction connections, and the like.

20 The locking guide wire 46 in combination with the attached guide wire handle  
56 and the alternative delivery cannulae 52 provides a very effective modular pedicle  
finder which can be used to facilitate the location and penetration of the pedicle of a  
25 vertebra. The advantageous use of the alternative delivery cannulae 52 in  
combination with such a modular pedicle finder provides the user with a device  
30 accessing the vertebral body by a transpedicular approach far superior to that known  
in the art. The positioning and direction of insertion of the guide wire 2, or locking  
guide wire 46 can be facilitated by using image guidance means such as fluoroscopy,  
35 CAT scan, MRI or the like. Stereotactic methods and the employment of registration  
diodes can also be employed to provide accuracy in guide wire insertion when the  
20 process of the invention is practiced from any approach to the vertebral body,  
including the use of the locking guide wire 46 to perform a transpedicular approach to  
the vertebral body. It is also within the concept of the present invention to employ  
45 robotic systems to control the accuracy of the insertion of the device.

As best shown in FIG. 9D, one alternative embodiment of the guide wire  
25 handle 56 can be provided with a removable proximal end 72. The removable

5 proximal end 72 permits the user to expose the proximal end of the guide wire for ease in movement, insertion, and extraction from the delivery cannulae. The removable proximal end 72 of the guide wire handle 56 can be releasably secured to the guide wire handle 56 by any known releasable connection means, such as, for 10 example, threaded connections, snap-fit connections, cotter-pin connections, friction connections, and the like. FIG's. 9E-F show examples of some of the alternative end attachments which can be employed with the alternative embodiment of the guide wire handle shown in FIG. 9D. Any configuration for the removable proximal end 72 that provides a gripping surface for the user is within the concept of the present 20 invention. Preferred alternative embodiments of the removable proximal end 72 are the spherical or oval gripping surface 76 (FIG. 9E) and the T-handle form 78 (FIG. 9F). Alternative handles which can be used with the present invention includes the cannulated T-handle shown in FIGS. 9G-H. FIG. 9I provides a partial sectional view of one embodiment of the present invention utilizing another option for the removable 30 proximal end 72, that of a removable impact extension member 72a. This optional member enables the user to attach an impact surface which surrounds and protects the guide wire if impacting the device is necessary during operation.

35 FIG'S 10A-C show details of an alternative plunger assembly 80 which can have a removable gripping member 82, which is secured by a removable lock pin 84 or similar securing member. The alternative plunger assembly 80 with the gripping 40 member 82 removed can be configured to an automated impelling means (not shown) much like automated infusion devices, which are known in the art. With the alternative plunger assembly 80 so configured, the degree of pressure applied to the plunger assembly in moving the material through the material conduit can be 45 automatically controlled by the user to avoid over pressurizing the material into the 25

5 spaces within the bone. The plunger assembly can be manufactured with a lock pin  
84, which is not removable. So configured, the plunger assembly would essentially  
be that of the earlier described unitary plunger member 32.

10 FIGS. 10D-J provide depictions of alternative embodiments of the present  
5 invention, which can use a standard threaded plunger and cannulae (FIGS. 10D-E) or,  
as shown in FIGS. 10F-G a long-threaded or optional mixing-tip plunger. Such  
15 embodiments of the present invention provide a controlled insertion of the plunger  
and an inherent resistance to any back pressure from the material being injected  
through the device. FIGS. 10H-J depict alternative handles which can be used with  
20 any of the earlier described embodiments of the present invention; particularly those  
shown in FIGS. 10D-G. The swivel ball gripping member 82a can be used to provide  
25 ease of movement of the plunger; particularly one of the threaded plungers depicted in  
FIGS. 10D-G.

30 FIG 11A shows a hand operated plunger actuator 86, which can be used to  
15 assist in the impelling of the material through the material conduit 14 of the present  
invention. FIG. 11B shows a type of syringe 42 which can be used to contain the  
material for use in the method of the present invention, the syringe being an example  
35 of the type syringe which can be used with the hand operated plunger actuator shown  
in FIG. 11A. Other impelling devices can also be used to assist in the movement of  
20 the material into the material conduit 14 without departing from the concept of the  
present invention.

45 The present invention also contemplates the use of an intraosseous injection  
device similar to the embodiments described above with the alternative modification  
of providing lumens which incorporate rifling along the bore of the lumen which can  
25 be of assistance to the user in enabling the ease of material insertion and allowing the

5 escape of air or other fluids of less consistency than that of the material being infused  
into the body. The tolerances between the plunger assembly 32 or 80 and the sides of  
the material conduit 14 are such that the material is easily forced through the conduit  
10 without loss of the material around the plunger, yet air or other light consistency  
5 fluids within the material conduit 14 are allowed to pass away from the body around  
the plunger to freely escape.

15 It is also within the concept of the present invention to provide an intraosseous  
injection device which has multiple lumens for passage of the material into the body,  
thus allowing for the possibility of mixing of material components at the time of  
20 injection. A multi-lumen device 116 such as that shown in FIGS. 11C-E can be used  
in a variety of situations, to include, for example, when it is desirable to withhold  
25 mixing of injectable material components as long as possible prior to injecting the  
mixed components into a subject. As best shown in FIG. 11E, the device can be  
provided with a separate plunger 118a, 118b for each lumen; the plungers being  
30 15 configured such that they can be operated independently or can be operated together  
by apply pressure to the overriding handle of one of the plungers 118a.

35 FIG. 12A shows an application of the method of the present invention, which  
employs a flexible delivery cannulae 88 for delivery of a material into the bone  
material of a joint, such as, for example into the acetabulum 90. A sealing washer 92  
40 20 can be provided to assist in maintaining the delivery cannulae 88 in place at the point  
of entry into the bone. FIG. 12B is an enlarged cross-sectional depiction of the  
flexible cannulae shown in FIG. 12A showing an example of a mechanism which can  
45 be employed to steer the flexible delivery cannulae 88. FIG 12B depicts a steering  
wire system 94, which employs at least two steering wires 96, one end of each  
25 steering wire being attached at the delivery cannulae distal end 98 in opposition one to

5 the other and the other end of the respective steering wires being attached in  
opposition one to the other to a rotary reel control 100 located adjacent to the Luer  
10 lock of the delivery cannulae. The steering wire system 94 described herein and  
shown in FIG. 12B is provided as an example of a steering system which can be used  
5 in the present invention. It is, however, within the concept of the present invention to  
employ any of the known means of producing a steerable catheter.

15 Also provided is a specialized impact forceps 102, as shown in FIG's. 13A-B.  
The specialized impact forceps can be used in conjunction with the device of the  
present invention for purpose of facilitating the entry of the device into the bone. The  
20 impact forceps 102, are operated by a user much like surgical forceps known in the  
art. A hinge member 104 connects the opposing halves 106a and 106b of the forceps  
allowing the halves 106a and 106b to be closed tightly together. A forceps lock 108  
25 allows the halves 106a and 106b to be locked into a closed position. Unique to the  
specialized forceps of the present invention is a first groove 110 and a second groove  
30 112 found in the end of the forceps which is tightly closed when the forceps is in the  
closed and locked position. The first groove 110 is sized and configured to securely  
35 grasp the guide wire element 2, which is sized to fit the first clearance hole 62 of the  
guide wire handle. The second groove 112 is sized and configured to securely grasp  
an impact connector element 64, which is sized to fit the second clearance hole 66 of  
40 the guide wire handle. The forceps 102 can have a striking plate 114, which is  
configured to receive driving blows from an operator using a mallet, hammer, spring-  
loaded driver, or other impacting device. In combination, the forceps 102 and the first  
45 clearance hole 62 can be used to facilitate driving the guide wire 46 into position in  
the bone. Similarly, the forceps 102 and the second clearance hole 66 can be used to  
25 facilitate driving the delivery cannulae into position.

5 In its most general form, the surgical procedure of the present invention  
includes the step of the physician, by tactile sensation, recognizing the appropriate  
back-pressure on the plunger gripping member and thereafter ceasing the manual  
10 introduction of injectable material into the cancellous bone. It is, however, within the  
scope of the present invention to provide a back-pressure sensor attached to the device  
1 such that when the preselected back-pressure on the plunger member is reached, the  
15 physician is apprised of the situation and introduction of material can be discontinued.  
It is further, within the scope of the present invention for the alternative embodiment  
which provides for automatic infusion of the biomaterial through the device 1, to  
20 provide a processor which receives a back-pressure signal at a preselected back-  
pressure and in turn transmits a pressure cut-off signal to the automatic infusion  
25 system.

The injection device of the present invention can be fabricated from any of a  
variety of materials, which are compatible for use as surgical instruments. Examples  
30 of such materials include metallic materials and non-metallic materials, which are  
suitable for use in surgical instrument manufacturing processes. Metallic materials  
can include, for example, surgical instrument grade stainless steel and alloys thereof,  
35 anodized aluminum and alloys thereof, and titanium and alloys thereof to include  
nickel-titanium. Non-metallic materials can include, for example, thermoplastics,  
40 ceramic materials, carbon fiber materials, composite materials, and the like.

It is within the scope of the present invention to provide a kit, which includes  
the injection device disclosed above. The kit could also include some or all of the  
45 alternative features discussed herein, to include the injectable material. Such a kit  
could be provided in an appropriate packaging, which could be designed for  
25 autoclaving or other means of sterilization.

5 In operation, the user can insert the guide wire 2 using a posterior lateral approach to the vertebral body. This can be safely done with the patient under general or local anesthetic.

10 The surgical procedure of the present invention can be performed by direct vision, open or percutaneously, laproscopically, thorascopically, or by open surgical procedures. Performance of the surgery percutaneously is preferred. A very important feature of the present invention is the ability to perform the surgical procedure percutaneously by a posterior-lateral approach in addition to the transpedicular approach. The use of a postero-lateral approach is preferred over the transpedicular approach because the physician can quickly, effectively and, most importantly, safely perform a vertebroplasty without bringing any instruments within close proximity to the spinal cord. Alternatively, the method of the present invention can be performed using a transpedicular approach with the limited bone penetration and accuracy of employment aspects of the present invention providing improved safety over conventional transpedicular approaches.

15 The surgical procedure is also easily adapted to be performed on any vertebrae from T3 down, which also represents a major expansion of applicability over the convention methods used.

20 Additionally, the procedure has been shown to be useful in fixing vertebral bodies which have tumors to the extent that the tumors have not caused the formation of holes in the compact bone of the vertebrae adjacent to the spinal cord.

25 Of major importance is the very limited degree of penetration of the guide wire 2 through the compact bone of the vertebrae. Unlike conventional vertebroplasty, which requires CAT scanning to precisely control drilling using a conventional vertebroplasty apparatus through the pedicle (see FIG'S 14 and 15), the



5 present invention can be more efficiently, and more quickly accomplished being aided  
only by the use of fluoroscopy. FIG. 14, shows the angle relative to the spinal  
column for transpedicular approaches using the conventional vertebroplasty apparatus  
10 and the conventional procedure of deeply penetrating into the cancellous bone of the  
vertebral body. The preferred posterior-lateral approach to the vertebra by the guide  
wire 2 and the penetration of the tapered end, which need only penetrate the compact  
15 cortical bone of the vertebral body, results in the cancellous bone of the vertebra  
being left in tact. In the alternative transpedicular approach of the present invention  
the transpedicular approach angle is similar to conventional methods, however, the  
20 improved control of depth of penetration of the apparatus of the present invention  
provides greater accuracy and therefore greater safety over conventional apparatus  
and methods. It is well known in the art, as evidenced by the discussion in Gray's  
Anatomy, 38<sup>th</sup> Ed. (1995) at page 427 and 454, that the relatively thin-walled exterior  
compact bone derives powerful support from the trabeculae of cancellous bone  
30 located within. Conventional vertebroplasty drills through and penetrates well into  
the cancellous bone of the vertebrae (see FIG. 15), thus severely disrupting the natural  
internal reinforcing structure of the vertebra. In the preferred embodiment of the  
35 present invention the guide wire 2 does not penetrate through the cancellous bone and  
therefore does not radically disrupt the trabeculae of the cancellous bone.. The result  
40 is that when the bone cement is introduced through the material conduit 14 of the  
delivery cannulae 12, it flows into the naturally porous configuration of the intact  
cancellous bone thus taking advantage of, not replacing, the natural internal  
45 supporting trabeculae structure of the vertebra.

As depicted in FIG. 16, In a first embodiment of the process of the present  
25 invention the vertebra are infused with bone cement using an entry port on one side

5 only of the vertebra. This unilateral infusion process does not completely fill the  
porous structure of the natural matrix of the cancellous bone; but fills it sufficiently on  
one side to fully support the failed vertebra.

10 As depicted in FIG. 17, in an alternative embodiment of the process of the  
5 present invention the surgery can be done as a bilateral procedure by first infusing the  
failed vertebra from one side and then repeating the entire process from the opposite  
15 side of the vertebra. By such a bilateral approach, it is possible for the physician, if he  
desires, to substantially fill all of the porous structure of the cancellous bone of the  
20 vertebra.

10 As depicted in FIG. 18, a further alternative embodiment of the process of the  
present invention could include the step of extending the guide wire 2 further into the  
25 cancellous bone of the vertebra and thus positioning the material conduit 14 of the  
delivery cannulae 12 more central to the cancellous bone portion of the vertebrae. As  
the porous structure of the cancellous bone is infused with bone cement using this  
30 alternative process, the delivery cannulae 12 can be slowly withdrawn from the  
15 cancellous bone structure while continuing to infuse the bone with bone cement. The  
result would be a substantially filled vertebrae using a unilateral process.

35 It should be known that while the surgical process of the present invention  
described above is particularly appropriate to provide fixation of vertebral  
40 20 compression failures due to osteoporosis, tumor or other pathogenic bone conditions,  
the process can also be used in cases of trauma induced compression failures.

45 Further, it is possible that the process could be used as a preventive or protective  
measure that could conceivably be used for patients, which present themselves as  
being extremely likely to suffer vertebral compression failures.

## Claims

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5           What we claim is:

1.       An injection device comprising:

10           a delivery cannulae having a proximal end and a distal end, which are  
connected by a cannulae body, and a lumen capable of acting as a material conduit,  
said lumen passing from said proximal end through said distal end;  
15           an elongated plunger, said plunger being sized and configured to slidably pass  
through said lumen;  
20           a removable handle configured for secure attachment to said proximal end of  
said delivery cannulae, said delivery cannulae being equipped with a handle retention  
member integrally formed in said proximal end of said delivery cannulae.

25       2.       An injection device according to claim 1, further comprising:

30           an elongated guide wire, said guide wire having a first end and a second end  
connected by an elongated guide wire body, said first end being configured with a  
taper, said taper being capable of breaching cortical bone sufficient to form a channel  
through said cortical bone; and  
35           an aligning cannulae having a gripping end and a tapered end, said aligning  
cannulae being sized and configured to slidably pass circumferentially over said guide  
40           wire and said delivery cannulae being sized and configured to slidably pass  
circumferentially over said aligning cannulae.

45       3.       An injection device according to claim 2, wherein said guide wire comprises  
graduated indicia on said guide wire body.

- 5           4.     An injection device according to claim 2, wherein said delivery cannulae  
comprises graduated indicia on said cannulae body.
- 10           5.     An injection device according to claim 2, wherein said plunger comprises a  
first end having a gripping member, said first end being connected by a plunger body  
15     to a second end having a blunt smooth tip, said gripping member comprising a swivel  
joint axially aligned with said plunger.
- 20           6.     An injection device according to claim 2, wherein said second end said guide  
wire comprises a gripping member.
- 25           7.     An injection device according to claim 2, wherein said aligning cannulae  
comprises a textured surface on said blunt end.
- 30           8.     An injection device according to claim 2, wherein said delivery cannulae  
comprises a securing edge on said distal end.
- 35           9.     An injection device according to claim 2, wherein said plunger comprises a  
plunger gripping member connected by a plunger body to a blunt smooth tip end.
- 40           10.    An injection device according to claim 2, further comprising a syringe system  
connected to said delivery cannulae and in fluid communication with said delivery  
45    cannulae lumen.
- 50
- 55

5 11. An injection device according to claim 10, wherein said syringe system is  
removably connected to said delivery cannulae by a connector selected from the  
10 group consisting of a Luer lock, a bayonet fitting, and a hydraulic quick disconnect  
fitting.

15 12. An injection device according to claim 11, wherein said connector is integral  
with said proximal end of said delivery cannulae and is aligned with the longitudinal  
axis of said delivery cannulae body.

20 13. An injection device according to claim 10, wherein said syringe system is  
connected to said delivery cannulae by a flexible conduit.

25 14. An injection device according to claim 2, wherein said guide wire comprises  
an attached longitudinally aligned a Luer lock connector.

30 15. An injection device according to claim 14, wherein said handle comprises a  
Luer lock configured to releasably engage said Luer lock connector of said guide  
35 wire, said handle further comprising a longitudinally aligned lumen opening at each  
end of said handle.

40 16. An injection device according to claim 11, wherein said connector of said  
delivery cannulae is a Luer lock and said handle comprises a Luer lock configured to  
45 releasably engage said Luer lock connector of said delivery cannulae, said handle  
further comprising a longitudinally aligned handle lumen opening at each end of said

5 handle, said handle lumen being in fluid communication with said lumen of said  
delivery cannulae.

10 17. An injection device according to claim 16, wherein said handle further  
comprises a view slot sized and configured to permit viewing of the handle lumen.

15 18. An injection device according to claim 16, wherein said handle further  
comprises a first clearance hole passing through said handle perpendicular to said  
20 handle lumen, said first clearance hole being sized and configured to slidably receive  
said guide wire.

25 19. An injection device according to claim 18, wherein said handle further  
comprises a second clearance hole passing through said handle perpendicular to said  
handle lumen, said second clearance hole being sized and configured to slidably  
30 receive said aligning cannulae.

35 20. An injection device according to claim 16, wherein said handle further  
comprises a removable proximal Luer lock end.

40 21. An injection device according to claim 10, wherein said syringe system  
comprises an automated impelling unit.

45 22. An injection device according to claim 21, wherein said automated impelling  
unit being capable of controlling the rate and amount of movement of the mechanism  
50 of said syringe system.

5

23. An injection device according to claim 22, wherein said automated impelling unit further comprises a pressure sensing unit.

10

15

24. An injection device according to claim 2, wherein said device is formed of materials selected from the group consisting of stainless steel, anodized aluminum, thermoplastics and glass.

20

25. An injection device according to claim 2, wherein said delivery cannulae lumen comprises multiple lumens.

25

26. An injection device according to claim 1, further comprising:  
an elongated guide wire, said guide wire having a first end and a second end connected by a elongated guide wire body, and said first end being configured with a taper, said taper being capable of breaching cortical bone sufficient to form a channel through said cortical bone, wherein said delivery cannulae is sized and configured to slidably pass circumferentially over said guide wire.

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27. An injection device in combination with an injectable material comprising:  
an elongated guide wire, said guide wire having a first end and a second end connected by a elongated guide wire body, and said first end being configured with a taper, said taper being capable of breaching cortical bone sufficient to form a channel through said cortical bone;

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5 an aligning cannulae having a gripping end and a tapered end, said aligning  
cannulae being sized and configured to slidably pass circumferentially over said guide  
10 wire;

a delivery cannulae having a proximal end and a distal end, which are  
connected by a cannulae body, and a lumen capable of acting as a material conduit,  
15 said lumen passing from said proximal end through said distal end, said delivery  
cannulae being sized and configured to slidably pass circumferentially over said  
aligning cannulae;

20 an elongated plunger, said plunger being sized and configured to slidably pass  
through said lumen;

25 a removable handle configured for secure attachment to said proximal end of  
said delivery cannulae, said delivery cannulae being equipped with a handle retention  
member integrally formed in said proximal end of said delivery cannulae; and

30 an injectable material provided to said lumen of said delivery cannulae, said  
injectable material being of a consistency such that upon controlled movement of said  
plunger, said injectable material will flow through said lumen.

35  
28. An injection device according to claim 25, wherein said injectable material is  
selected from the group consisting of bone cement, antibiotics, cellular implants,  
40 natural products of cells recombinant nucleic acid products, protein products of  
recombinant cells.

45  
29. An intraosseous injection device comprising:

an elongated guide wire, said guide wire having a first end and a second end  
50 connected by a elongated guide wire body, and said first end being configured with a

5 taper, said taper being capable of breaching cortical bone sufficient to form a channel through said cortical bone;

10 an aligning cannulae having a gripping end and a tapered end, said aligning cannulae being sized and configured to slidably pass circumferentially over said guide wire;

15 a delivery cannulae having a proximal end and a distal end, which are connected by a cannulae body, and a lumen capable of acting as a material conduit, said lumen passing from said proximal end through said distal end, said delivery cannulae being sized and configured to slidably pass circumferentially over said aligning cannulae;

20 an elongated plunger, said plunger being sized and configured to slidably pass through said lumen;

25 a removable handle configured for secure attachment to said proximal end of said delivery cannulae, said delivery cannulae being equipped with a handle retention member integrally formed in said proximal end of said delivery cannulae.

30 30. A method of introducing an injectable material into a subject, the method comprising:

35 introducing a delivery cannulae to a delivery site of a subject, wherein said delivery site is within a bone or adjacent to a bone; and

40 inserting material through said delivery cannulae into said delivery site, wherein said inserting step is accomplished by activation of a plunger being moved within said delivery cannulae.

5  
31. A method of introducing an injectable material into a subject, the method comprising:

10 introducing a guide wire through the cortical bone of a subject;  
introducing a delivery cannulae, circumferentially over said guide wire until  
said delivery cannulae contacts said cortical bone, said delivery cannulae having a  
15 lumen extending the length of said delivery cannulae;  
removing said guide wire from the subject;  
infusing an injectable material into said lumen; and  
20 infusing said injectable material into the bone of said subject by movement of  
a plunger within said lumen, said plunger being sized and configured to force said  
injectable material through said lumen while permitting air from within said lumen to  
25 escape proximally past said plunger.

30 32. A method of introducing an injectable material into a subject, the method comprising:

introducing a guide wire through the cortical bone of a subject;  
35 introducing an aligning cannulae circumferentially over said guide wire until  
said aligning cannulae contacts said cortical bone;  
introducing a delivery cannulae having a lumen circumferentially over said  
40 aligning cannulae until said delivery cannulae contacts said cortical bone;  
removing said guide wire and said aligning cannulae from the subject;  
45 infusing an injectable material into said lumen, and infusing said injectable  
material into the bone of said subject by movement of a plunger, said plunger being  
sized and configured to force said injectable material through said lumen of said

5 delivery cannulae while permitting air from within said lumen to escape proximally past  
said plunger.

10 33. A method according to claim 31, wherein said guide wire introducing step is  
into the body of a vertebra of the subject via an approach selected from the group  
15 consisting of postero-lateral approach, unilateral approach, bilateral approach and  
lateral intracortical bone penetration approach.

20 34. A method according to claim 31, wherein said guide wire introducing step is  
into the body of a vertebra of the subject via a transpedicular approach.

25 35. A kit for introducing an injectable material into a subject, the kit comprising:  
an injection device according to claim 1; and  
30 an injectable material selected from the group consisting of bone cement,  
antibiotics, whole cellular implants, natural products of cells, recombinant nucleic  
products and protein products of recombinant cells.

35 36. A kit according to claim 34, wherein said injectable material is  
polymethylmethacrylate.

40 37. A kit according to claim 34 further comprising:  
45 a syringe for connection to said injection device; and  
a container for enclosing said kit, said container being packaged for sterile  
delivery and suitable for off-the-shelf use.

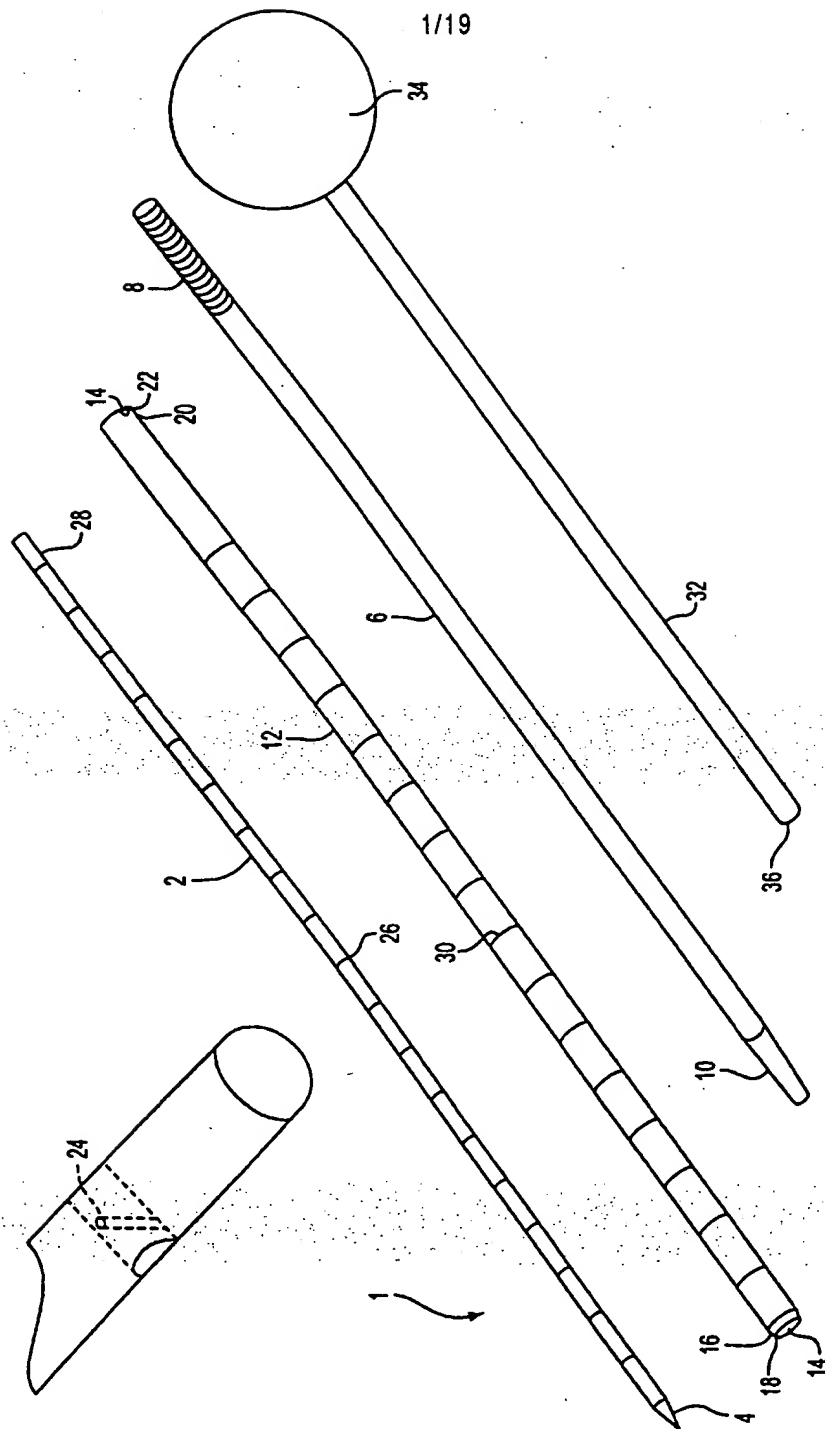
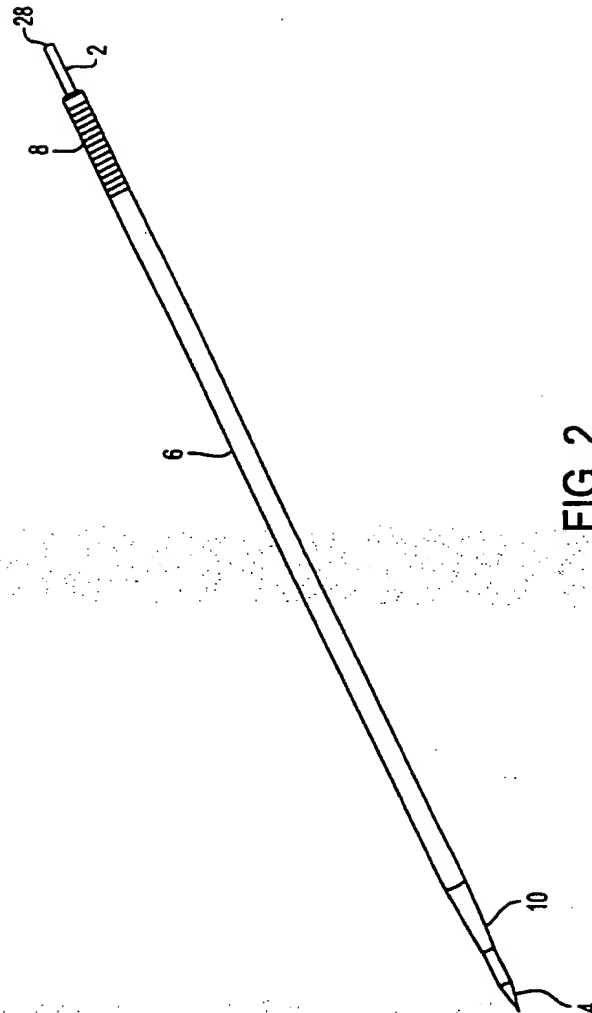


FIG. 1



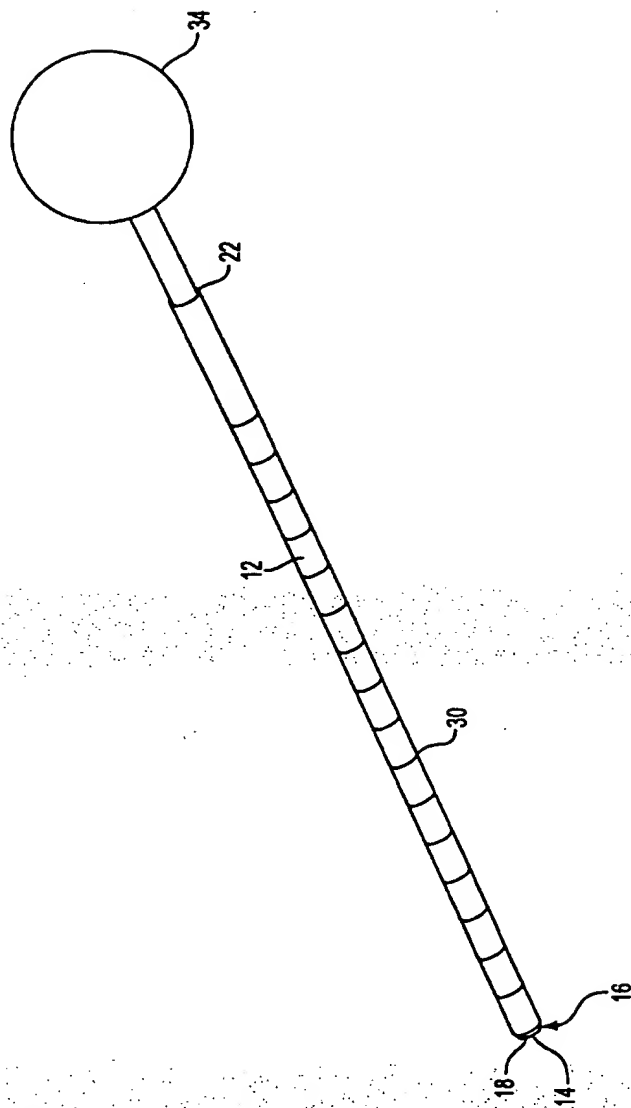
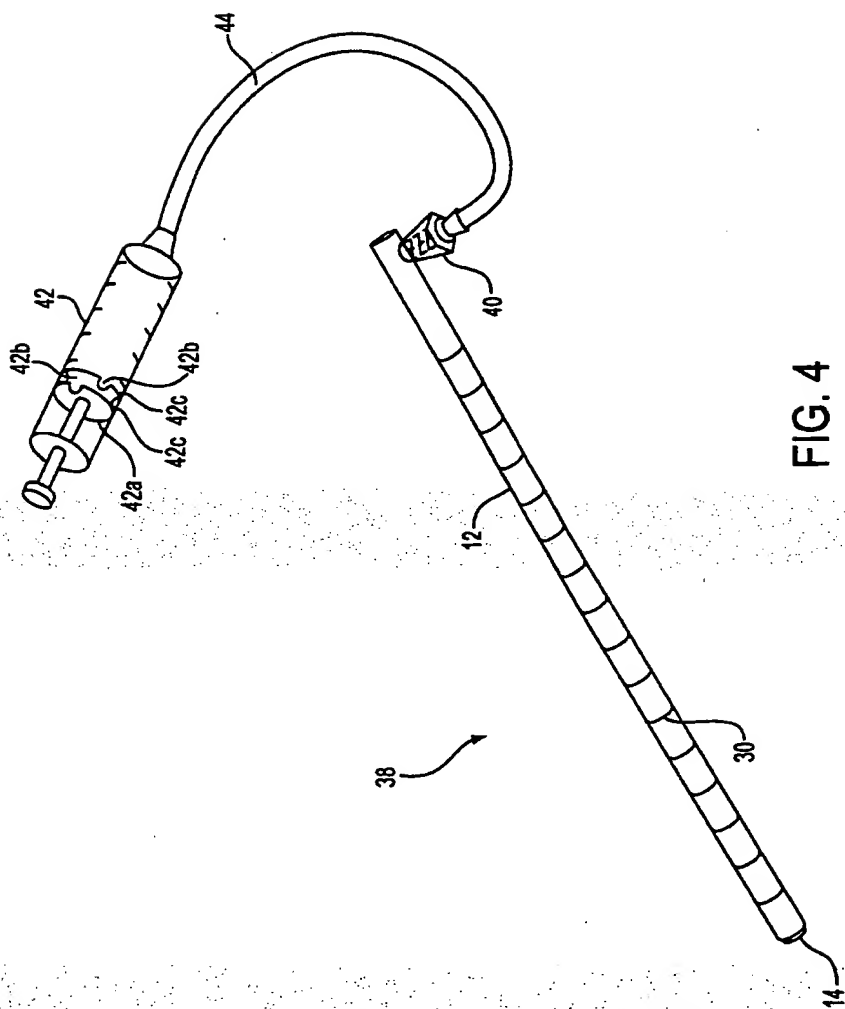
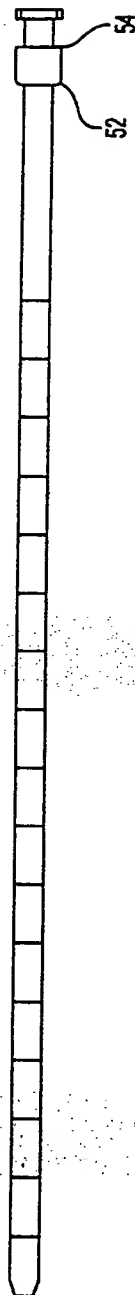
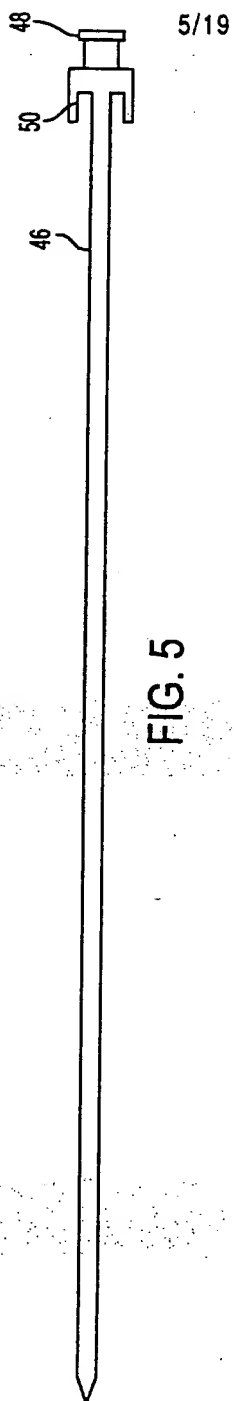


FIG. 3







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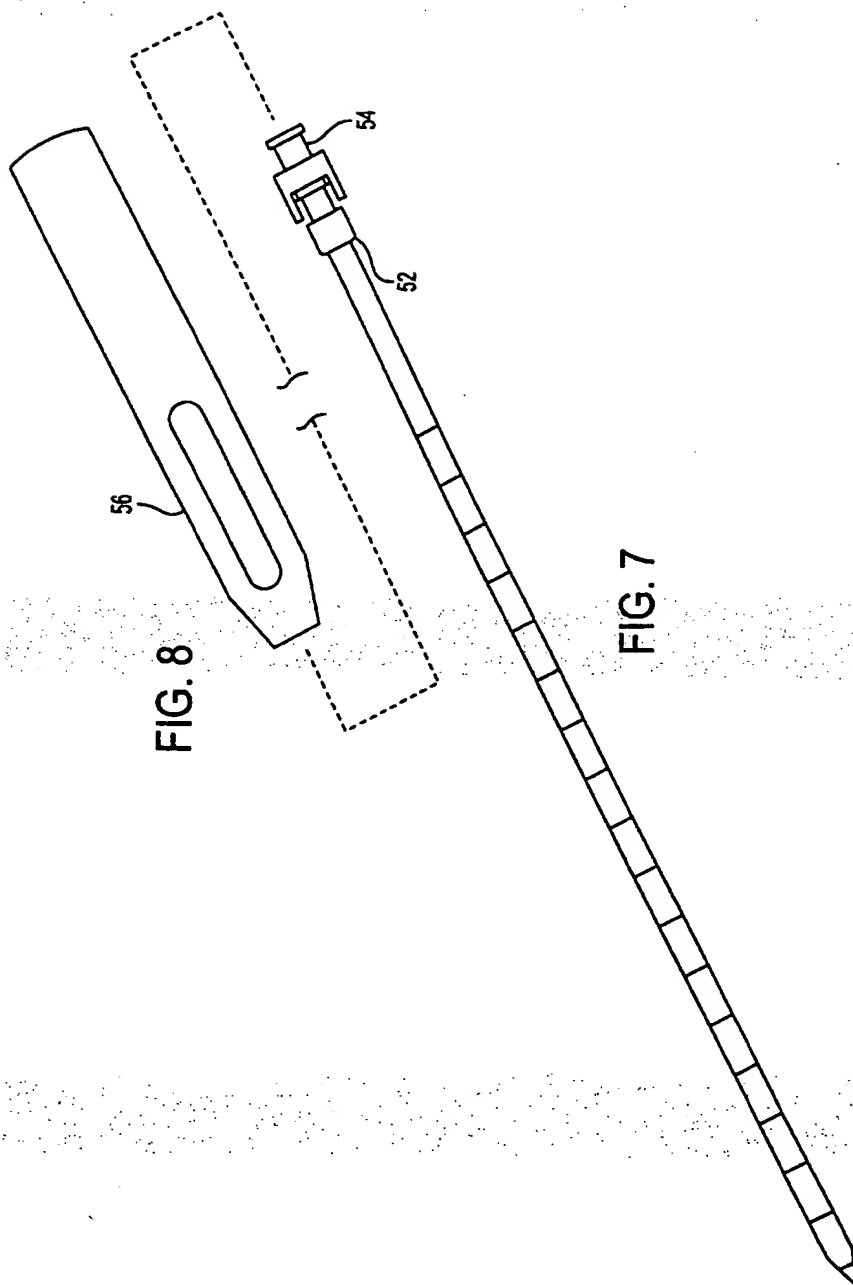


FIG. 8

FIG. 7

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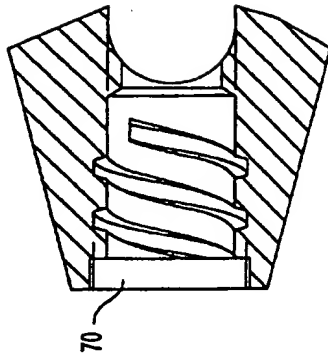


FIG. 9B

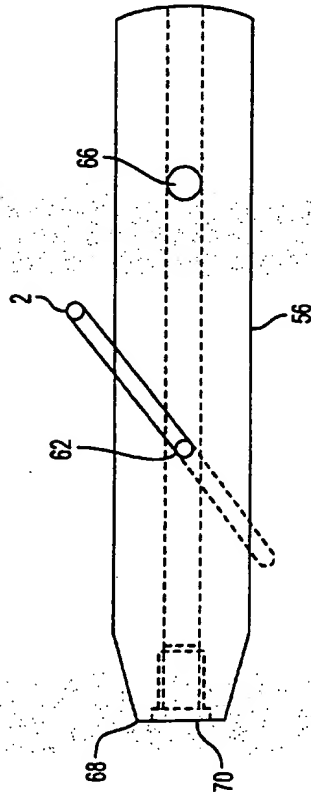


FIG. 9A

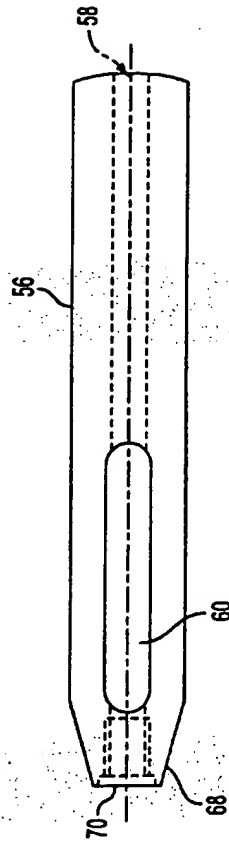


FIG. 9C

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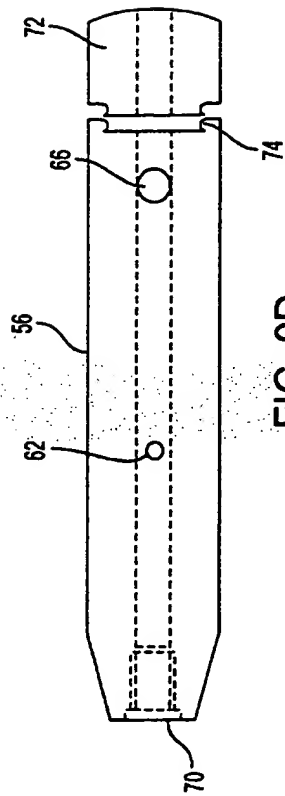


FIG. 9D

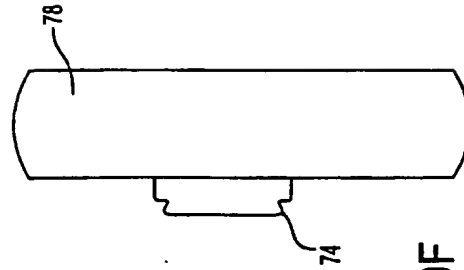


FIG. 9F

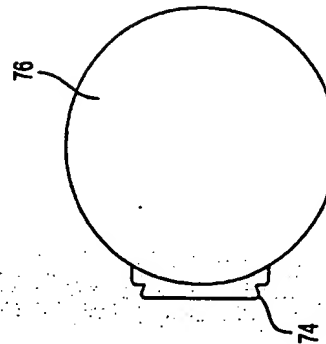


FIG. 9E

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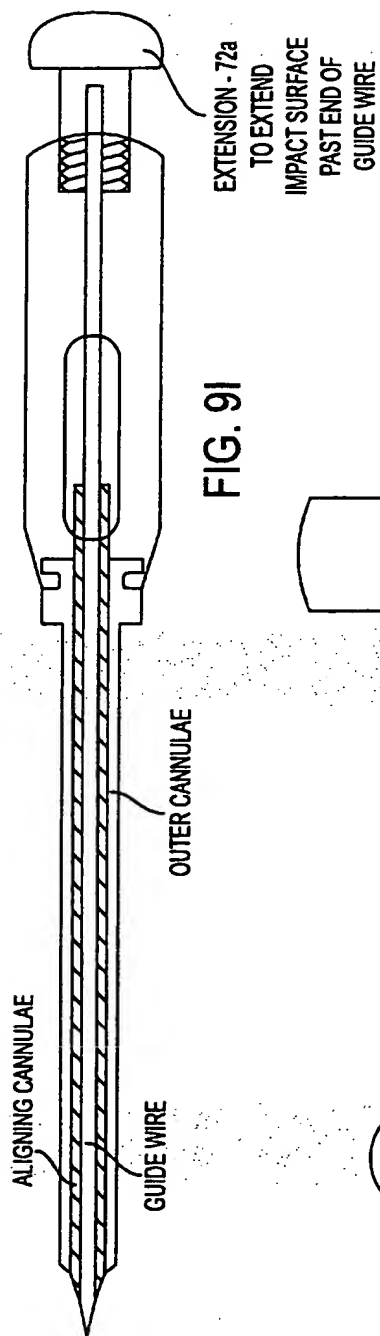


FIG. 9I

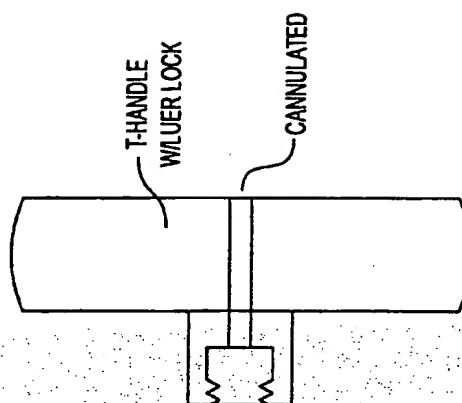


FIG. 9H

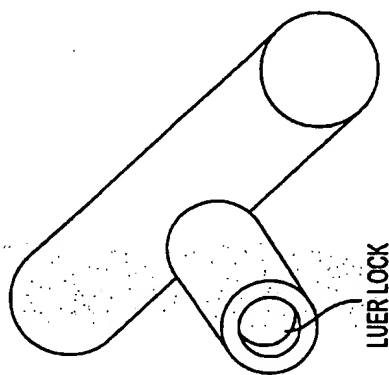


FIG. 9G

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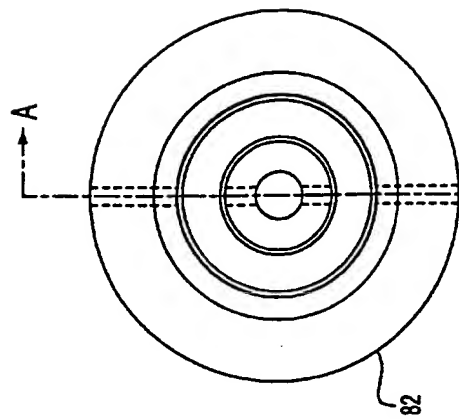


FIG. 10B

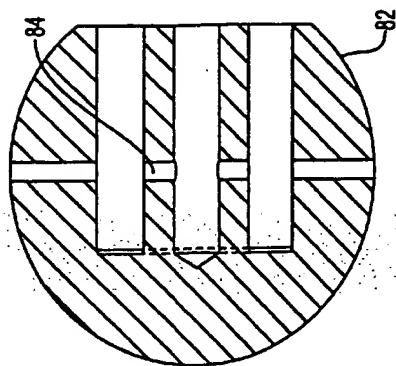
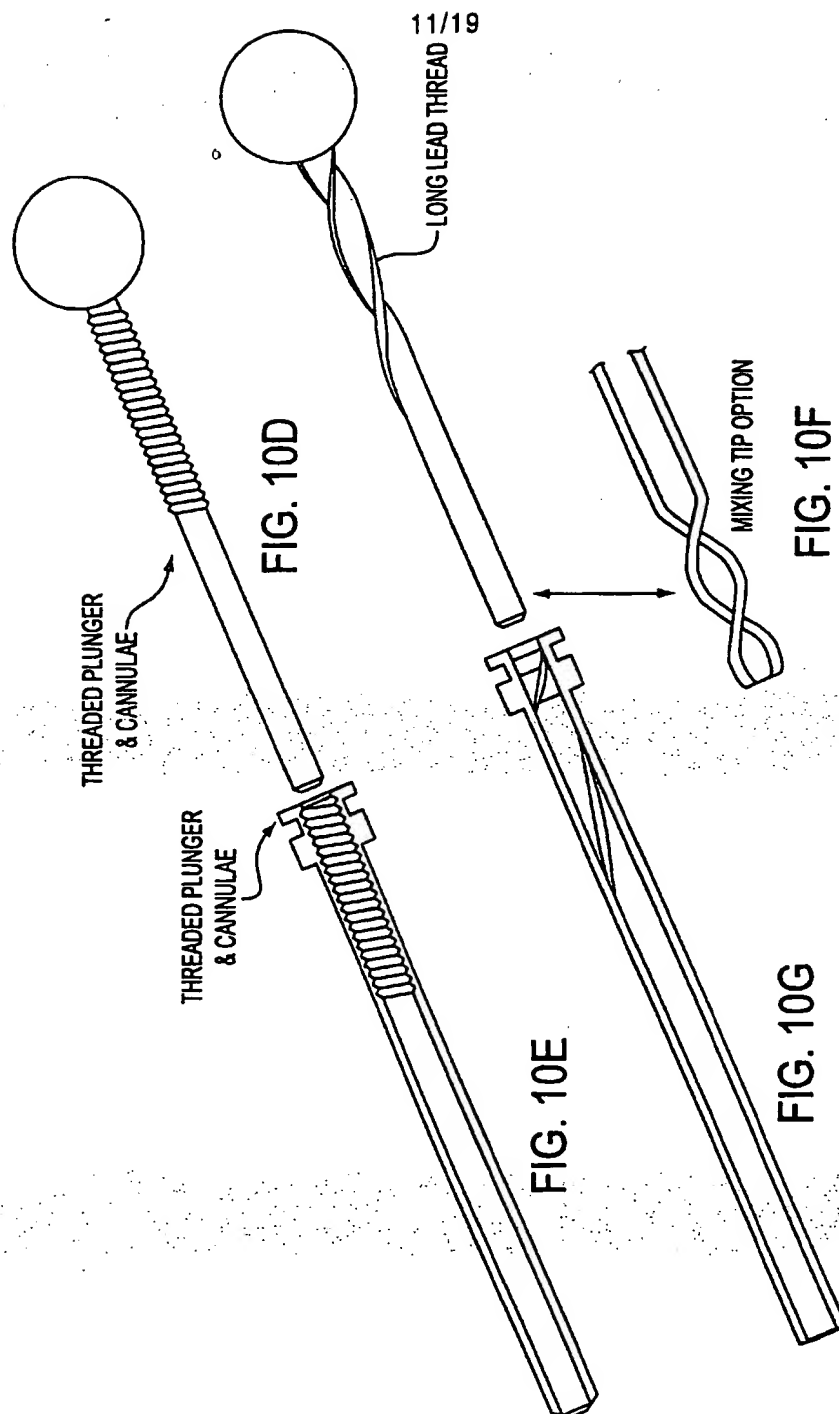


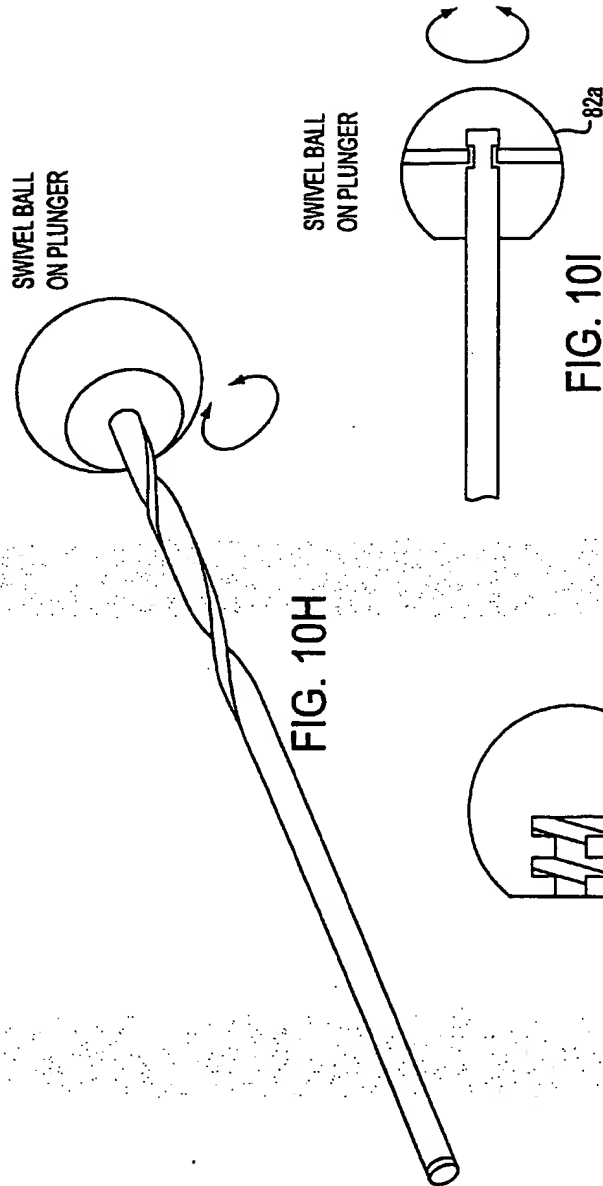
FIG. 10A



FIG. 10C



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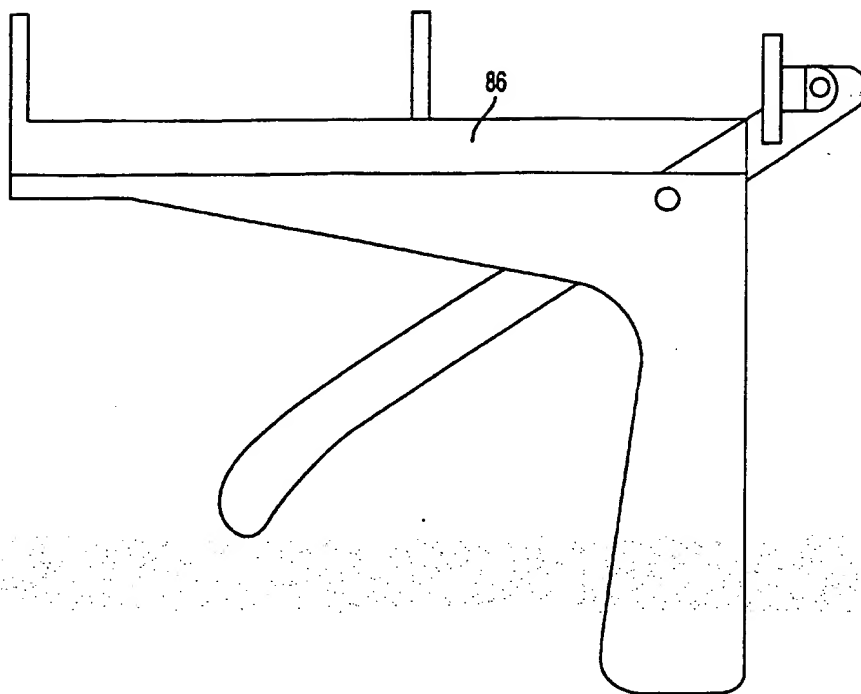


FIG. 11A

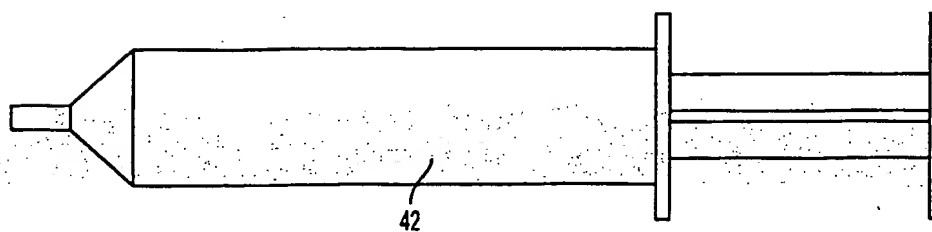


FIG. 11B

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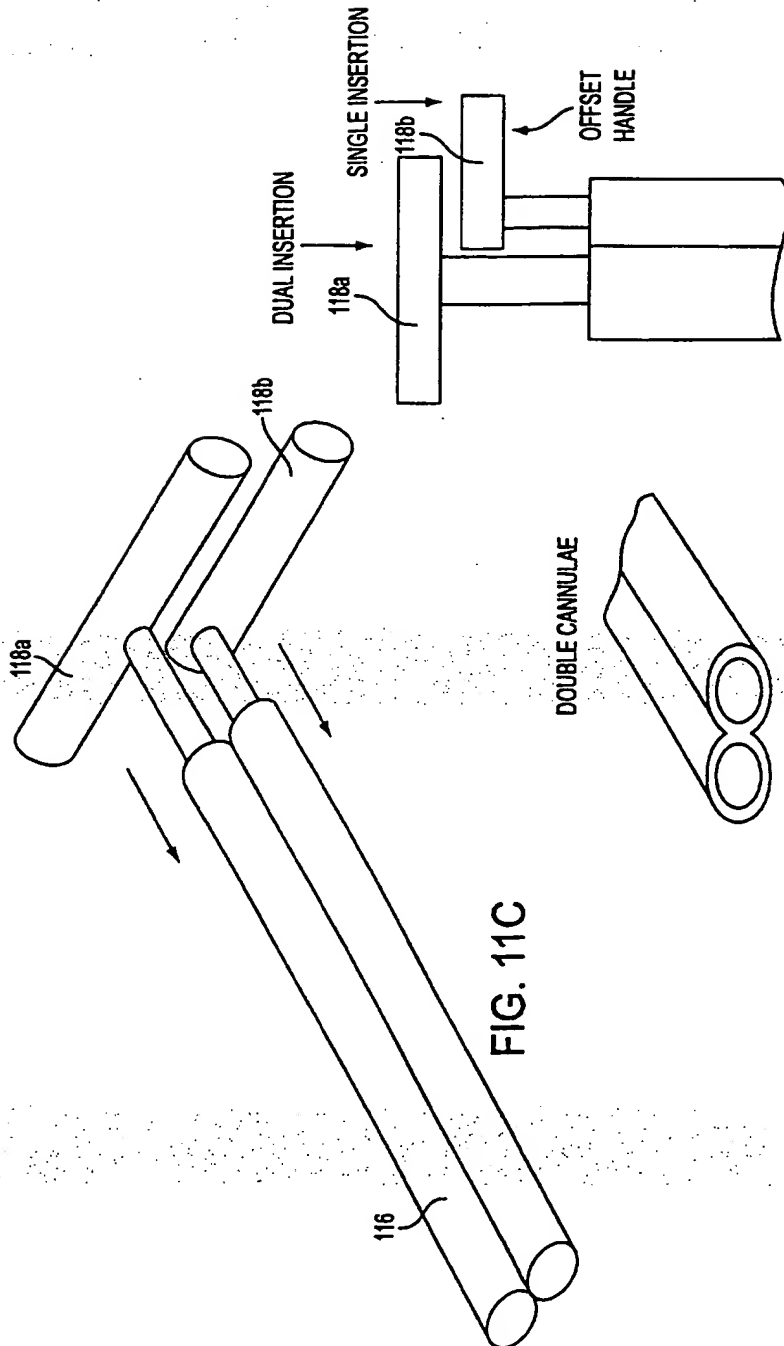
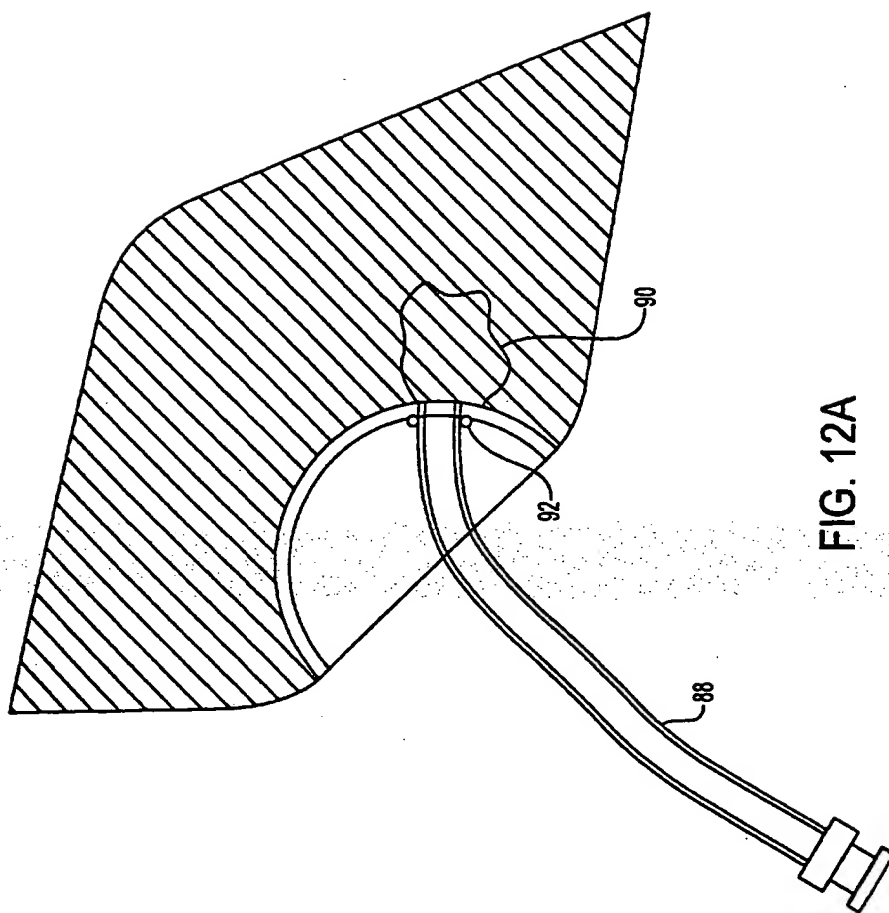


FIG. 11E

FIG. 11D

FIG. 11C





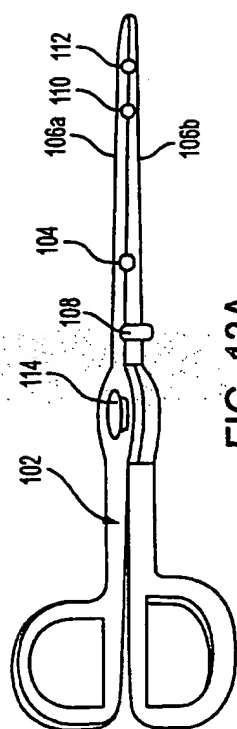


FIG. 13A

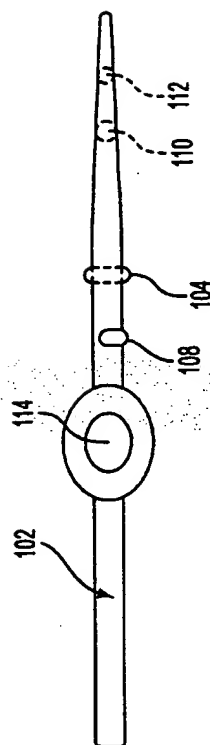


FIG. 13B

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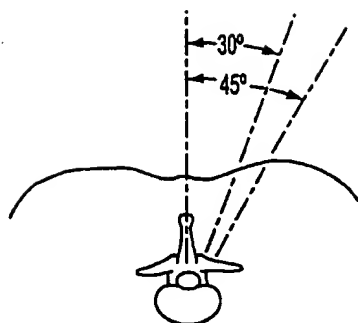


FIG. 14  
PRIORART

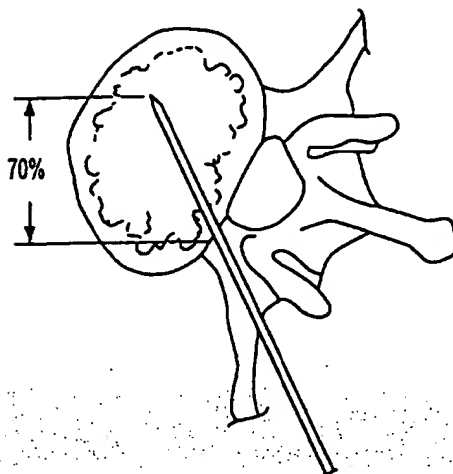


FIG. 15  
PRIORART

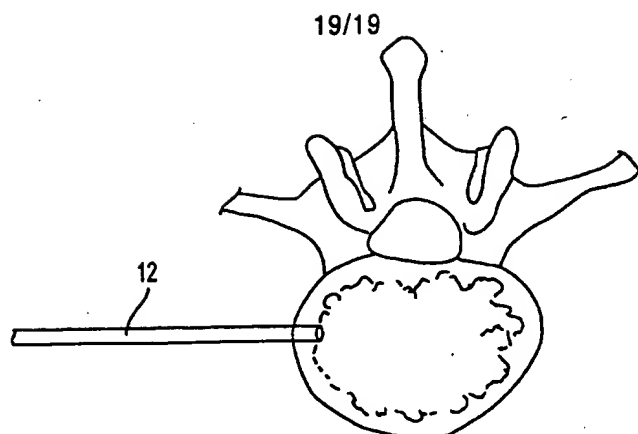


FIG. 16

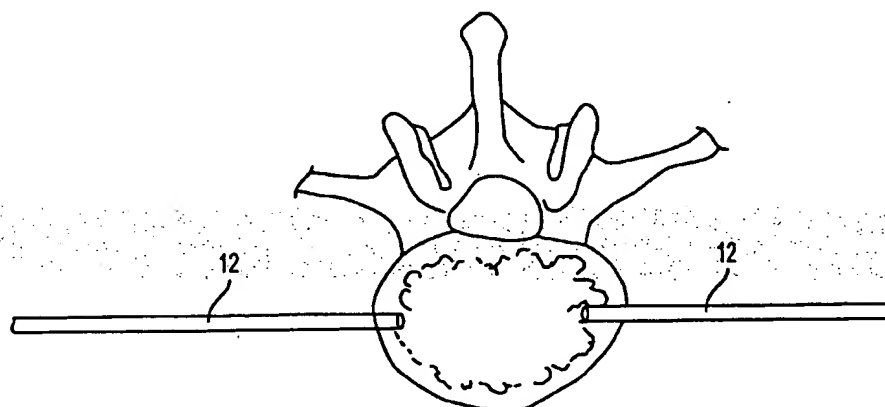


FIG. 17

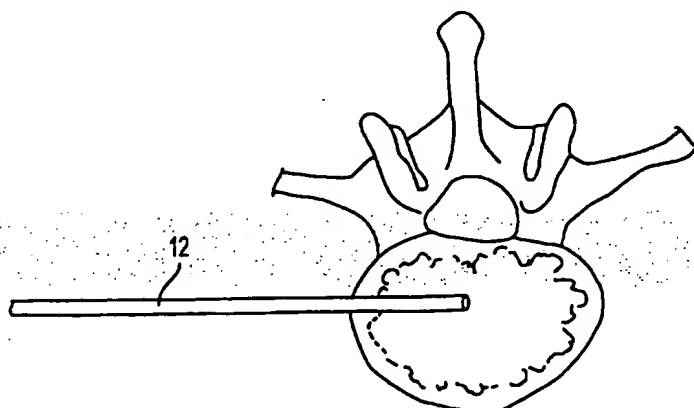


FIG. 18

# INTERNATIONAL SEARCH REPORT

International Application No.  
PCT/US 00/06643

<b>A. CLASSIFICATION OF SUBJECT MATTER</b> IPC 7 A61F2/46 A61B17/34				
According to International Patent Classification (IPC) or to both national classification and IPC				
<b>B. FIELDS SEARCHED</b> Minimum documentation searched (classification system followed by classification symbols) IPC 7 A61F A61B				
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched				
Electronic data base consulted during the international search (name of data base and, where practical, search terms used) EPO-Internal				
<b>C. DOCUMENTS CONSIDERED TO BE RELEVANT</b>				
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.		
Y	US 5 741 261 A (MOSKOVITZ PETER A ET AL) 21 April 1998 (1998-04-21)  column 13, line 41 - line 59; figure 20	1,5-12, 16, 27-29, 35-37		
Y	WO 90 04364 A (COOK INC ;UNIV FLORIDA (US)) 3 May 1990 (1990-05-03)  page 6, line 30 -page 7, line 23 page 8, line 10 - line 33 page 10, line 7 - line 15; figures 1-4	1,5-12, 16, 27-29, 35-37		
A	US 5 108 404 A (REILEY MARK A ET AL) 28 April 1992 (1992-04-28) cited in the application the whole document	1,2,10, 27,29,35		
-/-				
<input checked="" type="checkbox"/> Further documents are listed in the continuation of box C. <input checked="" type="checkbox"/> Patent family members are listed in annex.				
* Special categories of cited documents : <table border="0"> <tr> <td style="vertical-align: top;">           "A" document defining the general state of the art which is not considered to be of particular relevance            "E" earlier document but published on or after the international filing date            "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)            "O" document referring to an oral disclosure, use, exhibition or other means            "P" document published prior to the international filing date but later than the priority date claimed         </td> <td style="vertical-align: top;">           "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention            "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone            "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.            "S" document member of the same patent family         </td> </tr> </table>			"A" document defining the general state of the art which is not considered to be of particular relevance "E" earlier document but published on or after the international filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) "O" document referring to an oral disclosure, use, exhibition or other means "P" document published prior to the international filing date but later than the priority date claimed	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art. "S" document member of the same patent family
"A" document defining the general state of the art which is not considered to be of particular relevance "E" earlier document but published on or after the international filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) "O" document referring to an oral disclosure, use, exhibition or other means "P" document published prior to the international filing date but later than the priority date claimed	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art. "S" document member of the same patent family			
Date of the actual completion of the international search 28 June 2000		Date of mailing of the international search report 05/07/2000		
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentstein 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Tlx. 31 651 epo nl, Fax (+31-70) 340-3018		Authorized officer Hansen, S		



# INTERNATIONAL SEARCH REPORT

International Application No

PCT/US 00/06643

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5 824 087 A (ASPDEN RICHARD MALCOM ET AL) 20 October 1998 (1998-10-20) column 5, line 11 -column 6, line 24; figures 12-16	1,27,29, 35
A	DE 88 00 197 U (LIST H.-J.) 23 June 1988 (1988-06-23) claim 1; figures 1,2,4	1,3,4, 27,29,35

# INTERNATIONAL SEARCH REPORT

Information on patent family members

International Application No.

PCT/US 00/06643

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
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WO 9004364 A	03-05-1990	AT 116832 T	15-01-1995
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DE 8800197 U	23-06-1988	NONE	

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